

Review

# Artificial Intelligence and the Medical Physicist: Welcome to the Machine

Michele Avanzo <sup>1,\*</sup>, Annalisa Trianni <sup>2</sup>, Francesca Botta <sup>3</sup>, Cinzia Talamonti <sup>4</sup>, Michele Stasi <sup>5</sup> and Mauro Iori <sup>6</sup>

<sup>1</sup> Medical Physics Department Centro di Riferimento Oncologico di Aviano (CRO) IRCCS Aviano, 33081, Italy

<sup>2</sup> Medical Physics Unit, Ospedale Santa Chiara APSS, 38122 Trento, Italy; annalisa.trianni@apss.tn.it

<sup>3</sup> Medical Physics Unit, Istituto Europeo di oncologia IRCCS, 20141 Milan, Italy; francesca.botta@ieo.it

<sup>4</sup> Department Biomedical Experimental and Clinical Science “Mario Serio”, University of Florence, 50134 Florence, Italy; cinzia.talamonti@unifi.it

<sup>5</sup> Medical Physics Unit, A.O. Ordine Mauriziano di Torino, 10128 Torino, Italy; michele.stasi@unito.it

<sup>6</sup> Medical Physics Unit, Azienda USL-IRCCS di Reggio Emilia, 42122 Reggio Emilia, Italy; mauro.iori@ausl.re.it

\* Correspondence: mavanzo@cro.it

**Abstract:** Artificial intelligence (AI) is a branch of computer science dedicated to giving machines or computers the ability to perform human-like cognitive functions, such as learning, problem-solving, and decision making. Since it is showing superior performance than well-trained human beings in many areas, such as image classification, object detection, speech recognition, and decision-making, AI is expected to change profoundly every area of science, including healthcare and the clinical application of physics to healthcare, referred to as medical physics. As a result, the Italian Association of Medical Physics (AIFM) has created the “AI for Medical Physics” (AI4MP) group with the aims of coordinating the efforts, facilitating the communication, and sharing of the knowledge on AI of the medical physicists (MPs) in Italy. The purpose of this review is to summarize the main applications of AI in medical physics, describe the skills of the MPs in research and clinical applications of AI, and define the major challenges of AI in healthcare.

**Keywords:** artificial intelligence; deep learning; medical physicist; machine learning; big data

**Citation:** Avanzo, M.; Trianni, A.; Botta, F.; Talamonti, C.; Stasi, M.; Iori, M. Artificial Intelligence and the Medical Physicist: Welcome to the Machine. *Appl. Sci.* **2021**, *11*, 1691. <https://doi.org/10.3390/app11041691>

Academic Editor: Francesco Bianconi and Salvatore Gallo  
Received: 15 December 2020  
Accepted: 8 February 2021  
Published: 13 February 2021

**Publisher’s Note:** MDPI stays neutral with regard to jurisdictional claims in published maps and institutional affiliations.



**Copyright:** © 2021 by the authors. Licensee MDPI, Basel, Switzerland. This article is an open access article distributed under the terms and conditions of the Creative Commons Attribution (CC BY) license (<http://creativecommons.org/licenses/by/4.0/>).

## 1. Introduction

Artificial intelligence (AI) is a branch of computer science dedicated to giving machines or computers the ability to perform human-like cognitive functions, such as learning, problem-solving, and decision making [1,2]. AI-based systems have shown performance superior to experienced human beings in tasks, such as image classification and analysis, speech recognition, and decision-making [3]. Consequently, AI is expected to change profoundly every area of science, including medical physics, the clinical application of the principles of physics to healthcare [4,5]. The knowledge and skills of the medical physicists (MPs), which include aspects of mathematics, bioinformatics, statistics, safety, and ethics in the use of medical devices, are invaluable in the clinical and research applications of AI in medicine.

Moreover, analytical and computational techniques of physics, in particular those derived from statistical physics of disordered systems, can be extended to large-scale problems, including machine learning, e.g., to analyze the weight space of deep neural networks [6,7].

Given the exponential growth of applications of AI, such as machine learning (ML) and deep learning (DL) in all areas of medicine, which use ionizing radiation, ultrasounds, and magnetic fields for diagnostic and treatment purposes, witnessed over the past few years, the MPs’ workflow will be profoundly affected by the advent of AI. The areas affected will include quality controls of equipment, as linear accelerators and im-

aging devices, and software like diagnostic support systems [4,8] and decision support systems. The MPs will be more and more involved in the use of the new AI applications in medicine for patient diagnosis and treatment, with the primary scope of guaranteeing the quality of the whole process and environment [9].

The Italian Association of Medical Physics (AIFM) has created the AI for Medical Physics (AI4MP) task-group, with the aims of coordinating the efforts, facilitating the communication, and sharing of the knowledge on AI of the MPs in Italy. The aim of the present review is to summarize the point of view of the coordinators of AI4MP on the role and the involvement of MPs in the new AI world by defining the challenges of AI in healthcare for the MPs and by describing the skills the MPs can offer in this field. This will be done with a question in mind: if AI is welcomed by the MPs or vice versa.

## 2. Artificial Intelligence in Healthcare

**Machine learning (ML)** is the discipline that builds mathematical models and computer algorithms to perform specific tasks by learning patterns and inferences directly from data using computers, without being explicitly programmed to conduct these tasks [10]. ML algorithms can be either used for supervised learning, where the machine is provided with output labels to be associated with a set of input variables, or unsupervised learning. A popular supervised ML method is Support Vector Machines (SVM), which, by means of a kernel function, projects the data into a higher-dimensional feature space and determines a hyperplane in this feature space, which separates data points into categories [11]. Ensemble ML (EML) methods, such as Random forests or AdaBoost, are other supervised methods, which aggregate multiple learners, such as Decision Trees, into a single learner [12,13]. Naïve-Bayesian (NB) classifier calculates the probability of each class using the Naïve Bayes formula [14,15]. In unsupervised learning, the labels for given sets of input variables are not known, and the algorithm aims at finding correlations, patterns, or structures in the input variable space [16,17]. These include k-means clustering [18], principal component analysis (PCA) [19], Stochastic Neighbor Embedding (SNE) [20], and Laplacian eigenmaps [21].

**Deep learning (DL)** is a group of methods, which can be employed for supervised or unsupervised learning on any type of data, image, or signal. DL employs models with multiple stacks of neural layers to learn inherent patterns from input data and generate comprehensive representations, in contrast to classical ML methods, which use hand-crafted features manually extracted as input [2].

Nowadays, radiological and pathology images are stored, together with their reports, in picture archiving and communication systems (PACS). Besides, with the introduction of electronic health records (EHRs), systematic collections of patient health information have been made available, which include qualitative data, such as documents and records of patient demographics, medical records, and laboratory and diagnostics tests [22].

ML and DL, if applied to this large and often unstructured digital content, can determine information useful for epidemiological, clinical, and research studies [23,24]. Natural language processing (NLP) techniques, a combination of AI and linguistics, aimed at developing a computer's ability to understand human language [25], can be used to extract clinically relevant information from pathology and radiology reports [26], which can be integrated with features extracted from digital radiologic and pathology images stored in PACS [27].

The process used for these analyses is defined as "Data Mining". Data mining is used to find trends, patterns, correlations, anomalies, and features of interest in a database [28] in a data-driven inductive approach, which generates hypotheses from data [29]. Ideally, data mining necessitates the '4 V's' of 'Big Data'—volume, variety, velocity, and veracity of data. Instead of being used for prediction or diagnosis, in this case, ML is used to find clinically similar patients in the unstructured database, using all available

multimodal clinical data available, with the aim of discovering important groupings or defining features in the data [28].

Once similar patients are identified, the diagnosis, treatment, and outcome extracted from EHRs and other digital content can be ranked to give recommendations [17], e.g., by computerized clinical decision support systems (CDSS), which aid in decision-making [30]. In this way, pipelines can be designed to continuously and automatically extract information and improve the accuracy of patient outcome prediction [31].

### 3. Clinical Applications of Artificial Intelligence

#### 3.1. Imaging

The main purpose of the use of AI and ML applications in imaging is to support the specialist in the diagnosis of diseases. Computer-aided diagnosis (CAD) is among the first applications of these new algorithms in the imaging area [32,33] and incorporates ML classifiers trained to distinguish lesions from normal tissue [34]. In lung computed tomography (CT), ML applied to combinations of CT textural features scored high accuracy in distinguishing malignant lesions [35] or invasive from minimally invasive lesions [36].

In the relatively recent radiomics approach, quantitative analysis of radiological images (mainly CT [37–39], magnetic resonance imaging (MRI) [40–42], and positron emission tomography (PET) [43] images, but also ultrasounds [44], mammograms [45], and radiography) by extraction of a large number of image features (up to a few hundred or thousands) can be combined with ML classifiers to produce prognostic and predictive models [39].

In image elaboration, DL algorithms can learn the structure labeling of each image voxel directly (semantic segmentation) in order to contour lesions or organs [46]. U-net, one of the most popular DL architectures for image segmentation, has proven to be capable of automatically segmenting lung parenchyma [47] and lung tumor using PET-CT hybrid imaging [48].

A cornerstone of optimization of clinical imaging protocols is patients' dose estimation, which allows the dose to be balanced with image quality. Dose to the patient can be automatically calculated by DL in CT [49], single-photon emission computed tomography (SPECT) [50], and PET [51]. In interventional radiology, DL has been proposed for skin dose estimation [52]. In chest CT, ML could be used to predict the volumetric computed tomography dose index (CTDI<sub>vol</sub>) based on scan patient metrics (scanner, study description, protocol, patient age, sex, and water-equivalent diameter (DW)) and identify exams, which hold potential for dose reduction by tuning the acquisition parameters [53].

Another pillar of patient dose optimization is image quality improvement, as it allows dose reduction for the same image quality. The integration of AI algorithms within the imaging technology allows for improving imaging quality and, consequently, to reduce patient dose. DL methods have been used for improving PET image quality, reducing noise [54], removing streak artifacts from CT [55], and developing novel techniques for tomographic image reconstruction based on a reduced amount of acquired data. Other promising applications are a generation of synthetic images, such as synthetic CT from MRI [56], virtual contrast-enhanced images [57], and rigid/deformable intramodal and multimodal image registration [58], and extraction of the respiratory signal [21] that could be used for breathing motion compensation of images [59].

In interventional radiology, AI can predict tumor response to transarterial chemoembolization based on image texture and patient characteristics [60,61]. In the future, real-time registration DL algorithms could be used to superimpose high-resolution pre-operative MR imaging with intra-procedural fluoroscopy, guiding the physicians during the catheter's manipulation [62] for estimating ablation margins and helping minimize damages to structures close to the treated area.

AI can be useful also in longitudinal studies during follow-up of treatments in order to detect subtle changes between images, thus identifying progress or recurrence at an earlier stage [63,64]. Ophthalmic imaging, e.g., fundus digital photography, optical coherence tomography, among other imaging fields, is where artificial intelligence can support the specialist in the diagnosis of ophthalmic disorders, such as diabetic retinopathy, age-related macular degeneration, and others [65]. Other areas include cardiology [66,67] and rheumatology, which have a long history of research in AI applications aimed to detect and assess also rheumatological manifestations, bone erosions, and cartilage loss [68]. The development of digital pathology, due to the introduction of whole-slide scanners, and the progression of computer vision algorithms have significantly grown the usage of AI to perform tumor diagnosis, subtyping, grading, staging, and prognostic prediction. In the big-data era, the pathological diagnosis of the future could merge proteomics and genomics [69]. Spatial metabolomics is a new field aiming at measuring the distribution of molecules, such as metabolites, lipids, and drugs, within body structures, using imaging, such as mass spectrometry, where each pixel is represented by its mass spectrum [70]. Being characterized by a large amount of high dimensional data, including overlapping and noisy molecular signals, this technique looks promising for the application of AI [71].

Other applications that could become a focus of AI in the near future are computer vision [72], dealing with object detection and feature recognition in digital images, and virtual assistants [73], employing speech recognition in neuroradiology [74], radiology, and beyond. By augmented reality, the operator's perception of an operating room environment could be enhanced with AI-generated information [75].

### 3.2. Therapy

ML can be useful to carry out many of the activities during the whole workflow of radiotherapy, starting with the choice of the optimal radiation approach, e.g., choice of proton vs. photon [76]. A convolutional neural network (CNN) can automatically segment targets and organs at risk in radiotherapy [77]. ML-based auto-planning [78,79] mimics the iterative plan design, evaluation, and adjustments made by experienced operators with the goal of improving quality and efficiency and reducing inter-user variability [46]. Knowledge-based approaches leverage a large database of prior treatment plans (up to thousands) to develop associations between geometric and dosimetric parameters from a selection of previous plans in order to determine achievable dose constraints or dose distributions that can be used for benchmarking the quality of plans [9,80]. ML-based auto planning was also developed for brachytherapy [81].

The dose distribution from radiation therapy treatment can be predicted by DL in order to speed up the optimization [82] or determine the best achievable dose distribution from the patient image [83]. ML was applied to predict dose in brachytherapy [84] and in vivo measured dose in intraoperative radiotherapy [85].

Recently, dosomics, the application of radiomics or DL to the analysis of the dose distribution, eventually corrected into biologically effective dose to account for diverse fractionation, was investigated for the ability to predict side effects of radiation therapy [86,87]. Radiomics can also be applied to cone-beam CT (CBCTs) acquired for image-guidance of the radiotherapy treatment, making these images useful for data mining [88].

A major concern of radiotherapy is the change in the anatomy of the patient during therapy, which could result in unwanted dose changes. In this case, re-planning of the treatment is warranted. ML can identify significant changes in patient anatomy during radiotherapy [19] and predict patients who would benefit from adaptive radiotherapy (ART) [89]. Eventually, by using information extracted from radiomics voxel-based analyses, sensitive/resistant tumor sub-volumes might be identified, requiring higher (or lower) dose, thus enabling dose painting according to a "radiomic target volume" (RTV) [90].

In nuclear medicine, radiometabolic therapy with unsealed (radiopharmaceuticals) or sealed sources (microspheres, etc.) is of growing importance. The application of AI in this area can improve dosimetry by accounting for patients' anatomy, activity distribution, and tissue density, and planning, in order to administer the highest dose to the target while sparing critical organs, as well as for predicting treatment response [91]. Methodological studies have been performed to investigate the robustness of dosimetric approaches [92].

### 3.3. Quality Assurance (QA)

According to the International Organization for Standardization, QA is a system that ensures quality for a given product, service, process. Quality is the degree to which the system fulfills requirements (need or expectation that is stated—generally implied or obligatory) [93], thus avoiding mistakes and defects. Quality controls (QC) are the tests performed to describe, measure, analyze, improve, and control a certain product or process. In radiological sciences, QCs are applied to verify and monitor devices and procedures for diagnosis and therapy, as well as the support systems used by clinicians. AI can be used to perform automatically QCs that, if carried out manually, would not be feasible routinely due to a large amount of time required. AI QC systems could be used to learn and improve their accuracy over time and develop new tests over time without human intervention.

Quality assurance of radiotherapy (RT) is a significant part of the MP's work, and it is aimed at preventing radiological incidents and misadministration of radiation dose. A number of ML-based approaches have been explored to predict errors in treatment plans in order to automate chart check of plans. A K-means clustering algorithm was employed to learn from prior plans to perform the detection of errors in prostate plans [18].

Automated quality control of LINACs is another promising application of ML, which can be used for predicting machine performance issues, such as deviation of dose output [94], multileaf collimator (MLC) positions [95], and beam symmetry [96]. A method for automated quality control of LINACs by ML applied to electronic portal imaging device (EPID) was proposed, which could identify sag and deviations in the vertical direction and field shift [97]. Other AI applications aim at predicting results of in-phantom patients' specific QA of intensity modulated RT (IMRT) or volumetric modulated arc therapy (VMAT) [98,99].

## 4. Challenges and Pitfalls of AI

### 4.1. Data Size and Quality

ML and DL algorithms require a large amount of training samples, which grows rapidly with the dimensionality of data (the curse of dimensionality). An unappropriated data size will lead to a reduction in the certainty of the prediction, considering that many ML applications will always deliver a result, disregard the size and quality of the data set [100]. Unfortunately, a proper metric to evaluate sample size and power for ML and DL is missing.

Frequently, datasets used for training AI have a small number of samples with respect to the dimensionality of data and of the desired tasks [101], to the point that, frequently, there are more features per subject than subjects in the entire dataset [102]. Under these circumstances, overfitting, a condition where models are more sensitive to noise in the data than to their patterns, and instability occur, making the model poorly reproducible and generalizable, meaning that it will perform poorly on unseen datasets [103].

Feature selection algorithms, such as stepwise feature selection [104], the minimum redundancy maximum relevance (mRMR) [105], and RELIEF (relevance in estimating features) [106,107], can be applied to reduce overfitting by selecting a non-redundant subset of variables best suited to predict the outcome.

To reduce overfitting in DL, data augmentation (e.g., by the affine transformation of the images) during training is commonly implemented [10], and layers in the networks are specialized in reducing overfitting, such as dropout layers [108]. On the other side, DL suffers from other sources of uncertainties (e.g., the presence of many local minima in the loss function and the stochastic nature of training algorithms), so that repeating model training multiple times does not necessarily produce the same model [2]. Besides, the class imbalance problem, in which some classes have a significantly higher number of samples, is detrimental for ML performance, if not properly accounted for [109,110]. For overcoming class imbalance, under-sampling or over-sampling can be applied; the latter has been proven to be more effective [110].

Other biases in the training datasets, e.g., age, gender, and race, or in the diagnostic or therapeutical approach, e.g., technologies use for imaging or radiotherapy, may result in biased models, which may lead to poor performance for minority groups who are poorly represented in the training dataset. This could potentially aggravate healthcare disparities [103].

Another source of unreliability stems from the constant evolving of the patterns of clinical practice over time due to the introduction of new treatment approaches, technologies, or gradual changes in patient population (e.g., percentage of patients with a given histological subtype). This may result in increased unreliability of the AI system's recommendations or prediction over time [30]. The "half-life" of the relevance of clinical data used for training is thought to be typical of 4 months [111].

#### 4.2. Interpretability

Interpretability is the level of understanding of the information that the model extracts from input data, why it is extracted, and how it arrives at its output [2]. ML models are usually perceived as black boxes by the users and clinicians, meaning that they have a low level of interpretability. This issue is exacerbated for deep neural networks, given the complicated multi-layer structures and numerous numerical operations performed by each layer, and hinders the application of AI in the clinic.

Graph approaches can be of help to improve the interpretability of ML and DL methods. The activation maps extracted by the CNN, overlaid with the image analyzed, can show on which image regions the CNN focuses strongly for prediction [112]. For ML classifiers, interpretation can be facilitated by identification of the most important variables or features for prediction and comparing their values in illustrative cases, e.g., patients with a poor and good prognosis, as done in many radiomics studies, e.g., [86,113,114]. In unsupervised learning, some methods, like t-distributed stochastic embedding (t-SNE), allow visualization of high-dimensional data by giving each data point a location in a two or three-dimensional map [20].

#### 4.3. Legal and Ethical Issues

Key ethical issues associated with AI-systems automatically mining large patient databases include informed consent, privacy and data protection, ownership, objectivity, transparency of the obtained clinical or research model, and quality of training and validation data [115]. Automatizing tasks and decisions with the use of AI-based machines on a large scale could bring increased systemic risks of harm and systematic errors. These errors are categorized into omission when humans do not notice the failure of an AI tool and commission when an action is performed following AI's decision when there is evidence that AI is wrong [115]. The responsibility to prevent these errors by anticipating incorrect performance or misuses of AI before incidents occur falls to humans.

A model should be transparent, meaning that its formulas and code should be available and comprehensible so that it is possible to trace why an algorithm has failed and adverse clinical events [115]. The data "truthfulness" consists of understanding the type of information contained, the completeness and accuracy, their variance and bias, and if they reflect the problem of interest. Because of the "black box" phenomenon, in-

forming the patient clearly could become more difficult for the doctor when a decision is influenced by AI [116].

AI systems' decisions are based on the data used for training, the algorithms that are used, and what they have learned since their creation [117]. If some human biases, such as variability in healthcare because of ethnic, social, environmental, or economic factors, or clinically confounding factors, such as comorbidities, are present in the training data, they could result in biased decisions of the AI systems [28,117]. Since AI does not incorporate ethical concepts like equality, humans who use AI will hold the responsibility for preventing these errors [115]. Finally, before integrating AI into medical practice, it is important to prevent the loss of competence of the human who will not be able to carry out a task he used to do before because it has been transferred to the AI, also defined as "deskilling" [116].

## 5. Role of MP

### 5.1. Imaging

As already underlined in this paper, one of the major tasks in which the MP is deeply involved in the imaging field is the optimization process, i.e., finding the balance between dose and image quality.

MP understands the components of an imaging device used and the basic physical mechanisms at the root of signal change and image contrast and comprehends the technical and/or physiological artifacts limiting the performance [4,118]. Moreover, the MP understands the limitations and potential pitfalls of dose measurement, calculation, and prediction [90]. Thus, MP has knowledge and skills that are of value for the development, implementation, and use of AI in imaging.

AI-based systems have been developed to estimate patient dose. MP shall validate and periodically check these systems to avoid possible errors in the estimation. For example, the dose to each voxel in the calculated distribution depends on the dose calculation algorithm used, on the calculation voxel spacing, and on the uncertainty in dose measurement in the dataset used for ML training. In phantom, dose measurements can be planned by the MP to test algorithms' predictions.

MP shall also assess image quality through routine testing [119]. Recently, image quality enhancers, based on DL, have been introduced in clinical practice in order to ameliorate image quality. Consequently, image acquisition protocols could be updated to achieve dose reduction, and the MP will be involved in the optimization to ensure the minimum possible ionizing radiation dose to the patient [119,120].

It is also necessary to verify to what extent the imaging parameters' change influences the quantitative image content and, consequently, the response of AI systems. To this purpose, various physical phantoms have been developed. The Credence Cartridge Radiomics (CCR) phantom for radiomics was created for CT [121] and CBCT [122] images. More recently, anthropomorphic phantoms with heterogeneous objects were designed in order to simulate the texture of lung nodules [123]. PET phantoms with 3D printed inserts simulating heterogeneities in FDG uptake have been proposed [124], as well as MR phantoms simulating relaxation times and texture of pelvic tissue and malignancies [125]. Using these kinds of phantoms, the sensitivity of radiomics-based ML classifications on image acquisition parameters has been investigated. In CT, the classification is affected by the device used [121], method of image reconstruction [126], noise reduction algorithms, slice thicknesses [127,128]. PET features depend on acquisition mode [129,130], reconstruction algorithm, image resolution, and discretization [131,132]. MRI features are sensitive to the field of view, field strength, pulse sequence, reconstruction algorithm, and slice thickness [133].

Physical and digital phantoms could also be used to periodically verify the performances of image-based ML algorithms. Digital phantoms are usually representative scans of patients with known acquisition parameters. A dataset of CTs acquired twice on

the same patient 15 min apart allows “test-retest”, an assessment of the reproducibility of the radiomics workflow under the same conditions [127].

The accuracy of AI-generated segmentation, image reconstruction, and synthetic images (e.g., MRI) can be assessed using a ground truth digital phantom, for example of brain glioma patients [133] and image simulators, capable of simulating MRI acquired with different pulse sequence or field strength and reconstructed with different methods [133]. Specific tests allow assessing the accuracy of AI-based image registration [134].

In addition, MP can ensure correct extraction and quantitative analysis of imaging data. Thus, before performing quantitative analysis with AI algorithms, the accuracy and precision associated with the quantitative parameters within the images (e.g., tumors) should be assessed [29]. Moreover, MP is responsible for the pre-processing of images necessary for correct AI application. This would include the conversion of PET and SPECT images in standard uptake value (SUV), the standardization of MR images intensity scale [135], as well as assessment and correction of confounding factors of images, such as artifacts for metal implants in CT, magnetic field non-uniformity in MRI, and partial volume effect (PVE) in nuclear medicine images. Multimodal images should be registered using a proper method for rigid or deformable registration [136], a critical step that may affect the accuracy of AI models analyzing hybrid image datasets voxel by voxel [137] in order to combine metabolic, functional, and morphologic information.

In interventional radiology, MPs are involved in monitoring patients’ dose and manage patients’ radiation risks by reviewing interventional procedures [138]. The involvement of MPs will also reach safe implementation and QA of other AI systems, such as robotic angiographs and/or neuro-navigators, robots, etc., and platforms (catheter navigation assistants, analyzing relationships between catheter positions, therapeutic effect, and patient outcomes, etc.) for interventional therapies.

In other fields of medical imaging where AI is rapidly emerging, such as pathology imaging, MPs can support the acceptance and validation of AI systems. Recently, [139] pathology Digital Imaging and Communications in Medicine (DICOM) file format has standardized the representation, storage, and communication of pathology images acquired with whole-slide scanners [139]. Common acquisition protocols could reduce the variability in slide preparation and digitization procedures and scanner models among different centers and improve the performance of AI detection systems.

## 5.2. Data Collection and Curation

Given their skills in numerical analysis and clinical integration, MPs can significantly aid in the management of aggregate data [4], which will include clinical and image data from multiple modalities, such as PET, CT, radiography MRI, ultrasound, daily CBCT, hybrid imaging, such as PET/CT and PET/MRI, 3D/4D and image time series, and 3D/4D dose distribution from RT. MP will be involved in the development of metrics to assess the quality and completeness of data, methods to curate data, and QA programs of data archives [140].

CAD systems and other AI-based decision systems using images as input will need minimum quality specification and acquisition protocols in order to ensure output accuracy. The MP can ensure that the images are acquired according to the protocol required for correct AI use, free from relevant imaging artifacts, and correctly preprocessed [141] and harmonized [142] to reduce variability.

Moreover, MP can ensure that image data, together with their acquisition parameters and the dosimetric data from imaging and therapy, are stored in commonly accepted standards, such as the Digital Imaging and Communication in Medicine (DICOM), or comparable format and can create new standards for raw acquisition data to be stored in the standard format [143]. MP will necessarily oversee storage, security, and integrity of the large, machine-readable data collections needed to build a model [103]. The QA of datasets is a guarantee for the clinician, patient, and patient associations of the ethical and unbiased use of patients’ health data by AI systems.



### 5.3. Commissioning and Validation of AI

Commissioning of AI tools is a series of tests to assess if the system installed in the local site operates correctly and is ready for clinical use. The commissioning tasks, tests, schedule, and tolerances, with the required equipment and human resources, should be planned before installation [30]. The test plan could consist, for example, of applying AI to a set of well-known clinical cases, for which ground truth data are available. Comparison of different ML methods on the same dataset is useful and can show which ML algorithms have the best performance and which are more prone to overfitting data for the task at hand [85,144]. A technique called adversarial ML, where attempts to deceive models are carried out with a number of crafted configurations of data, e.g., by adding noise to images, can be used for quality assessment of many classes of ML and DL algorithms [145,146].

The lack of interpretability of AI systems—or ‘black-box’ problem—constitutes an obstacle towards their adoption in the clinic [10]. Monitoring AI performance by proper quality controls that test the models in well-known situations can improve the interpretability of models, as well as assessing architectures of DL models and their output using activation and feature maps.

An initiative led by the US FDA, the Microarray Sequencing Quality Control MAQC/SEQC [147], invites researchers to submit their models, features selected as important, and performance estimates to a specific data analysis plan (DAP), which includes ML and statistical crosscheck, before performing external validation data [100].

Validation, e.g., using the criteria in the TRIPOD statement [148], is required because many of the available AI models are trained using small datasets, and although augmentation and resampling methods are frequently applied, they are affected by overfitting and poor generalizability and reproducibility [112]. Large and possibly multi-institutional datasets, independent from the training datasets with realistic variability and the lowest bias as possible, are needed for validation. These can be achieved by increasing the level of collaboration among institutions [112], and the MP can play a role in checking the compliance with the required standards.

### 5.4. AI in Radiotherapy

MPs contributed to making radiotherapy into a frontier of personalized precision medicine by developing CT-based dose calculation, treatment planning, and image-guided radiation therapy (IGRT) [90]. Other traditional domains of MPs in radiotherapy include quality assurance and radiation protection [90]. MPs have been also at the forefront in using AI in RT, leading to the implementation of knowledge-based treatment planning, where ML algorithms are trained on the dataset, comprising patient images, contours, clinical information, and treatment plans performed by experienced MPs to automatically develop high-quality plans, allowing to accelerate radiotherapy plan design [46].

As with any other ML-based procedures, auto-planning systems also are as good as their human-generated training data, and their outcome will need to be tested and finally approved. Oftentimes, the proposed plan will need to be customized and modified by clinical MPs because of the unique anatomy of every patient. More importantly, when potential issues are identified for a specific plan, MPs communicate with other team members, such as physicians, therapists, and dosimetrists, to reach a clinically acceptable solution [149].

MPs are involved in validation and quality assurance of dose predicted by DL [90], which can be tested by properly designed in-phantom film/ion chamber measurements according to dosimetry protocols and benchmarking against previously established dose calculation algorithms. Another critical aspect is also investigating how the uncertainties of dose affect prognostic or predictive dosimetric models [90].

Given their familiarity with imaging devices and LINACs derived from managing QA programs, MP will have a critical role in the analysis of AI applied to the quality control of LINACs. When an AI tool predicts a machine failure, MPs can help identify the cause of the issue and corrective actions, such as calibrations [149].

#### 5.5. Safety/Risk Management

One of the key activities of the MP is patient safety management that is the evaluation of medical devices and procedures to guarantee the safety of patients. MPs are trained to prevent and analyze accidents [149] by using risk assessment, which consists of the analysis of events potentially involving accidental medical exposures or injury to a patient [150], and failure modes and effects analysis (FMEA) [151].

ML has the potential to reduce imaging radiation exposure, which is a hazard for patients and workers, without penalizing image quality [152].

#### 5.6. Periodical Tests

QA should be applied to AI systems themselves, which, having an impact on patient's health, should be considered as medical devices [153]. Physicists are also responsible for ensuring that clinically used AI algorithms continue to perform with the desired level of accuracy by conducting an appropriate routine QA test program with clearly established frequency, metrics, tolerance levels, and actions to be performed in case of test failure [103]. The frequency and nature of the series of tests will be in need of frequent updates, given the rapid pace of evolution of AI.

This is especially important for those AI systems that, being constantly learning and updating, will be subject to change in terms of their response and accuracy [94,119]. At the same time, it is critical to assess the effect of the decay of the relevance of the training data due to changes in practices (e.g., changes in prescribed dose and dose per fractions) [94].

#### 5.7. Training of AI Users

According to a white paper, the Canadian Association of Radiologists [154] should provide practitioners with an understanding of the value, the pitfalls, weaknesses, and potential errors that may occur in the use of AI products [154]. The medical physics associations are launching initiatives to provide appropriate training and education programs in the field of AI applied to imaging and therapy [90]. On the other hand, being skilled at communication and divulgation of science, MPs are critical to establishing a common language with other professionals and patients [155]; MPs can take part in education and training in the use of AI of other health care professionals, and be a part of the interdisciplinary team working for the effective, efficient, and safe delivery of AI in the clinic [3].

#### 5.8. Research in AI

MPs are often active researchers and, having expertise also in statistics, mathematics, and informatics, are suitable for research in AI. Extensive research is needed to understand how to successfully introduce AI and define the use and characteristics of AI in clinical practice [119].

Other active areas of research where MPs will be primarily involved include assessing data veracity and validity, developing metrics for completeness, accuracy, correctness, and consistency, and perform data cleaning activities [140]. Physicists should promote the integration of digital information from diagnostic and therapeutic procedures with genotyping and phenotyping data into large data sets acquisition across all areas (clinical, dosimetric, imaging, molecular, pathological, etc.), requiring multi-institutional and multinational collaboration [24,90]. Examples of this are The Cancer

Imaging Archive (TCIA) [156] and the Platform for Imaging in Precision Medicine (PRISM) platform [157].

The specific task for MPs in AI research includes the definition of the problem to be solved and determining its category (e.g., classification, regression, pattern recognition) in the lexicon of AI, choosing proper models to be trained, determining a strategy for collecting data from the appropriate dataset, and validating the model [103]. MPs also need to investigate and report the possible pitfalls of the AI-based methods developed and on how to overcome them. Besides, challenging is a personalizing therapy according to AI output, e.g., dose painting in radiotherapy [90].

Privacy, security, secure access to health information, de-identification of sensitive data, and obtaining informed consent, which are also of concern in research areas, become more relevant in the era of big data. The MP involved in these research areas will be required to apply the statements and recommendations released by governmental agencies, scientists, healthcare providers, companies, and other interested parties and will have an active role in formulating these statements [140].

Moreover, if MPs work at developing AI models or fine-tuning them on their data, they have to carefully understand and address the limitations of the data used for training and of the trained models [94]. Exploring multiple approaches, such as different feature selection and ML methods and their combinations, can help in understanding these limitations.

The Findability, Accessibility, Interoperability, and Reusability (FAIR) principles are intended to guide researchers into data management and reporting [158]. The methodology of research studies should be detailed thoroughly, including also deep learning architectures and optimization parameters, and the datasets used to train models should be clearly described in order to increase reproducibility and facilitate meta-analysis. Moreover, decision, automation, and prediction models relying on AI must be tested in independent and sufficiently large datasets to compare their validity against established methods, including conventional biomarkers (e.g., clinical, radiological, etc.). The codes and data used for training and testing the models should be made publicly available, e.g., by The Cancer Image Archive. More guidelines for improving transparency and reproducibility of models can be found in the TRIPOD [148].

## 6. Conclusions

AI can extend the expertise area of MPs, extracting even more information to improve patient care, and the MP is ready to welcome the AI revolution. On the other hand, the MPs' knowledge and skills will be required and beneficial for safe and optimal implementation of AI, especially in radiological sciences, and their involvement in the multidisciplinary AI team is crucial.

**Author Contributions:** Writing – Original Draft preparation: M.A., M.I.; Writing – Review & Editing: M.A., A.T., F.B., C.T., M.S., M.I. All authors have read and agreed to the published version of the manuscript.

**Funding:** This research was funded by the Associazione Italiana di Fisica Medica e Sanitaria (AIFM).

**Institutional Review Board Statement:** Not applicable.

**Informed Consent Statement:** Not applicable.

**Data Availability Statement:** Not applicable.

**Conflicts of Interest:** The authors declare no conflict of interest.

## References

1. Hashimoto, D.A.; Rosman, G.; Rus, D.; Meireles, O.R. Artificial Intelligence in Surgery: Promises and Perils. *Ann. Surg.* **2018**, *268*, 70–76.
2. Shen, C.; Nguyen, D.; Zhou, Z.; Jiang, S.B.; Dong, B.; Jia, X. An introduction to deep learning in medical physics: Advantages, potential, and challenges. *Phys. Med. Biol.* **2020**, *65*, 05TR01.
3. Xing, L.; Krupinski, E.A.; Cai, J. Artificial intelligence will soon change the landscape of medical physics research and practice. *Med. Phys.* **2018**, *45*, 1791–1793.
4. Samei, E.; Grist, T.M. Why physics in medicine? *Phys. Med.* **2019**, *64*, 319–322.
5. Samei, E.; Pawlicki, T.; Bourland, D.; Chin, E.; Das, S.; Fox, M.; Freedman, D.J.; Hangiandreou, N.; Jordan, D.; Martin, M.; et al. Redefining and reinvigorating the role of physics in clinical medicine: A Report from the AAPM Medical Physics 3.0 Ad Hoc Committee. *Med. Phys.* **2018**, *45*, e783–e789.
6. Biehl, M.; Caticha, N.; Oppen, M.; Villmann, T. Statistical Physics of Learning and Inference. In Proceedings of the European Symposium on Artificial Neural Networks, Computational Intelligence and Machine Learning, Bruges, Belgium, 24–26 April 2019.
7. Ramezanpour, A.; Beam, A.L.; Chen, J.H.; Mashaghi, A. Statistical Physics for Medical Diagnostics: Learning, Inference, and Optimization Algorithms. *Diagnostics* **2020**, *10*, 972.
8. Tang, X.; Wang, B.; Rong, Y. Artificial intelligence will reduce the need for clinical medical physicists. *J. Appl. Clin. Med. Phys.* **2018**, *19*, 6–9.
9. Thompson, R.F.; Valdes, G.; Fuller, C.D.; Carpenter, C.M.; Morin, O.; Aneja, S.; Lindsay, W.D.; Aerts, H.J.W.L.; Agrimson, B. C. Deville, C., Jr.; et al. Artificial intelligence in radiation oncology: A specialty-wide disruptive transformation? *Radiother. Oncol.* **2018**, *129*, 421–426.
10. Avanzo, M.; Wei, L.; Stancanello, J.; Vallieres, M.; Rao, A.; Morin, O.; Mattonen, S.A.; El Naqa, I. Machine and deep learning methods for radiomics. *Med. Phys.* **2020**, *47*, e185–e202.
11. Chen, S.; Zhou, S.; Yin, F.F.; Marks, L.B.; Das, S.K. Investigation of the support vector machine algorithm to predict lung radiation-induced pneumonitis. *Med. Phys.* **2007**, *34*, 3808–3814.
12. Avanzo, M.; Stancanello, J.; El Naqa, I. Beyond imaging: The promise of radiomics. *Phys. Med.* **2017**, *38*, 122–139.
13. Galar, M.; Fernandez, A.; Barrenechea, E.; Bustince, H.; Herrera, F. A Review on Ensembles for the Class Imbalance Problem: Bagging-, Boosting-, and Hybrid-Based Approaches. *IEEE Trans. Syst. Man, Cybern. Part C Applications Rev.* **2012**, *42*, 463–484.
14. Ben-Bassat, M.; Klove, K.L.; Weil, M.H. Sensitivity Analysis in Bayesian Classification Models: Multiplicative Deviations. *IEEE Trans. Pattern Anal. Mach. Intell.* **1980**, *PAMI-2*, 261–266.
15. Kukar, M.; Kononenko, I.; Silvester, T. Machine learning in prognosis of the femoral neck fracture recovery. *Artif. Intell. Med.* **1996**, *8*, 431–451.
16. Tseng, H.; Wei, L.; Cui, S.; Luo, Y.; Haken, R.K.T.; El Naqa, I. Machine Learning and Imaging Informatics in Oncology. *Oncology* **2020**, *98*, 344–362.
17. Syeda-Mahmood, T. Role of Big Data and Machine Learning in Diagnostic Decision Support in Radiology. *J. Am. Coll. Radiol.* **2018**, *15*, 569–576.
18. Azmandian, F.; Kaeli, D.; Dy, J.G.; Hutchinson, E.; Ancukiewicz, M.; Niemierko, A.; Jiang, S.B. Towards the development of an error checker for radiotherapy treatment plans: A preliminary study. *Phys. Med. Biol.* **2007**, *52*, 6511–6524.
19. Chetvertkov, M.A.; Siddiqui, F.; Kim, J.; Chetty, I.; Kumarasiri, A.; Liu, C.; Gordon, J.J. Use of regularized principal component analysis to model anatomical changes during head and neck radiation therapy for treatment adaptation and response assessment. *Med Phys.* **2016**, *43*, 5307–5319.
20. Maaten, L.v.d.; Hinton, G.E. Visualizing Data using t-SNE. *J. of Machine Learning Research* **2008**, *9*, 2579–2605.
21. Sanders, J.C.; Ritt, P.; Kuwert, T.; Vija, A.H.; Maier, A.K. Fully Automated Data-Driven Respiratory Signal Extraction From SPECT Images Using Laplacian Eigenmaps. *IEEE Trans. Med Imaging* **2016**, *35*, 2425–2435.
22. Groenhof, T.K.J.; Koers, L.R.; Blasse, E.; de Groot, M.; Grobbee, D.E.; Bots, M.L.; Asselbergs, F.W.; Lely, A.T.; Haitjema, S.; van Solinge, W.; et al. Data mining information from electronic health records produced high yield and accuracy for current smoking status. *J. Clin. Epidemiol.* **2020**, *118*, 100–106.
23. Gultepe, E.; Green, J.P.; Nguyen, H.; Adams, J.; Albertson, T.; Tagkopoulos, I. From vital signs to clinical outcomes for patients with sepsis: A machine learning basis for a clinical decision support system. *J. Am. Med. Inform. Assoc.* **2014**, *21*, 315–325.
24. Chamunyonga, C.; Edwards, C.; Caldwell, P.; Rutledge, P.; Burbery, J. The Impact of Artificial Intelligence and Machine Learning in Radiation Therapy: Considerations for Future Curriculum Enhancement. *J. Med Imaging Radiat. Sci.* **2020**, *51*, 214–220.
25. Pons, E.; Braun, L.M.; Hunink, M.G.; Kors, J.A. Natural Language Processing in Radiology: A Systematic Review. *Radiology* **2016**, *279*, 329–343.
26. Kreimeyer, K.; Foster, M.; Pandey, A.; Arya, N.; Halford, G.; Jones, S.F.; Forshee, R.; Walderhaug, M.; Botsis, T. Natural language processing systems for capturing and standardizing unstructured clinical information: A systematic review. *J. Biomed. Inform.* **2017**, *73*, 14–29.
27. Burger, G.; Abu-Hanna, A.; de Keizer, N.; Cornet, R. Natural language processing in pathology: A scoping review. *J. Clin. Pathol.* **2016**, *69*, 949–955.

28. Benke, K.; Benke, G. Artificial Intelligence and Big Data in Public Health. *Int. J. Environ. Res. Public Health* **2018**, *15*, 2796, doi:10.3390/ijerph15122796.
29. Castiglioni, I.; Gallivanone, F.; Soda, P.; Avanzo, M.; Stancanello, J.; Aiello, M.; Interlenghi, M.; Salvatore, M. AI-based applications in hybrid imaging: How to build smart and truly multi-parametric decision models for radiomics. *Eur. J. Nucl. Med. Mol. Imaging* **2019**, *46*, 2673–2699.
30. Mahadevaiah, G.; Rv, P.; Bermejo, I.; Jaffray, D.; Dekker, A.; Wee, L. Artificial intelligence-based clinical decision support in modern medical physics: Selection, acceptance, commissioning, and quality assurance. *Med Phys.* **2020**, *47*, e228–e235.
31. Welch, M.L.; McIntosh, C.; McNiven, A.; Huang, S.H.; Zhang, B.B.; Wee, L.; Traverso, A.; O'Sullivan, B.; Hoebbers, F.; Dekker, A.; et al. User-controlled pipelines for feature integration and head and neck radiation therapy outcome predictions. *Phys. Medica* **2020**, *70*, 145–152.
32. El Naqa, I.; Li, R.; Murphy, M.J. *Machine Learning in Radiation Oncology: Theory and Applications*; Springer: Berlin, Germany, 2015.
33. Giger, M.L.; Karssemeijer, N.; Schnabel, J.A. Breast image analysis for risk assessment, detection, diagnosis, and treatment of cancer. *Annu. Rev. Biomed. Eng.* **2013**, *15*, 327–357.
34. Elter, M.; Horsch, A. CADx of mammographic masses and clustered microcalcifications: A review. *Med. Phys.* **2009**, *36*, 2052–2068.
35. Chen, C.H.; Chang, C.K.; Tu, C.Y.; Liao, W.C.; Wu, B.R.; Chou, K.T.; Chiou, Y.R.; Yang, S.N.; Zhang, G.; Huang, T.C. Radiomic features analysis in computed tomography images of lung nodule classification. *PLoS ONE* **2018**, *13*, e0192002.
36. Weng, Q.; Zhou, L.; Wang, H.; Hui, J.; Chen, M.; Pang, P.; Zheng, L.; Xu, M.; Wang, Z.; Ji, J. A radiomics model for determining the invasiveness of solitary pulmonary nodules that manifest as part-solid nodules. *Clin. Radiol.* **2019**, *74*, 933–943.
37. Botta, F.; Raimondi, S.; Rinaldi, L.; Bellerba, F.; Corso, F.; Bagnardi, V.; Origgi, D.; Minelli, R.; Pitoni, G.; Petrella, F.; et al. Association of a CT-Based Clinical and Radiomics Score of Non-Small Cell Lung Cancer (NSCLC) with Lymph Node Status and Overall Survival. *Cancers* **2020**, *12*, 1432.
38. Cong, M.; Feng, H.; Ren, J.L.; Xu, Q.; Cong, L.; Hou, Z.; Wang, Y.Y.; Shi, G. Development of a predictive radiomics model for lymph node metastases in pre-surgical CT-based stage IA non-small cell lung cancer. *Lung Cancer* **2020**, *139*, 73–79.
39. Avanzo, M.; Stancanello, J.; Pirrone, G.; Sartor, G. Radiomics and deep learning in lung cancer. *Strahlenther. Onkol.* **2020**, *196*, 879–887.
40. Stanzione, A.; Gambardella, M.; Cuocolo, R.; Ponsiglione, A.; Romeo, V.; Imbriaco, M. Prostate MRI radiomics: A systematic review and radiomic quality score assessment. *Eur. J. Radiol.* **2020**, *129*, 109095.
41. Algohary, A.; Viswanath, S.; Shiradkar, R.; Ghose, S.; Pahwa, S.; Moses, D.; Jambor, I.; Shnier, R.; Bohm, M.; Haynes, A.M.; et al. Radiomic features on MRI enable risk categorization of prostate cancer patients on active surveillance: Preliminary findings. *J. Magn. Reson. Imaging* **2018**, *48*, 818–828.
42. Zhang, Z.; Yang, J.; Ho, A.; Jiang, W.; Logan, J.; Wang, X.; Brown, P.D.; McGovern, S.L.; Guha-Thakurta, N.; Ferguson, S.D.; et al. A predictive model for distinguishing radiation necrosis from tumour progression after gamma knife radiosurgery based on radiomic features from MR images. *Eur. Radiol.* **2018**, *28*, 2255–2263.
43. Hatt, M.; Tixier, F.; Visvikis, D.; Le Rest, C.C. Radiomics in PET/CT: More Than Meets the Eye? *J. Nucl. Med.* **2016**, *58*, 365–366.
44. Lee, S.E.; Han, K.; Kwak, J.Y.; Lee, E.; Kim, E.K. Radiomics of US texture features in differential diagnosis between triple-negative breast cancer and fibroadenoma. *Sci. Rep.* **2018**, *8*, 1–8.
45. Sapate, S.G.; Mahajan, A.; Talbar, S.N.; Sable, N.; Desai, S.; Thakur, M. Radiomics based detection and characterization of suspicious lesions on full field digital mammograms. *Comput. Methods Progr. Biomed.* **2018**, *163*, 1–20.
46. Jarrett, D.; Stride, E.; Vallis, K.; Gooding, M.J. Applications and limitations of machine learning in radiation oncology. *Br. J. Radiol.* **2019**, *92*, 20190001.
47. Skourt, B.A.; El Hassani, A.; Majda, A. Lung CT Image Segmentation USING Deep Neural Networks. *Procedia Comput. Sci.* **2018**, *127*, 109–113.
48. Zhong, Z.; Kim, Y.; Zhou, L.; Plichta, K.; Allen, B.; Buatti, J.; Wu, X. 3D fully convolutional networks for co-segmentation of tumors on PET-CT images. In Proceedings of the 2018 IEEE 15th International Symposium on Biomedical Imaging (ISBI 2018), Washington, DC, USA, 4–7 April 2018; pp. 228–231.
49. Peng, Z.; Fang, X.; Yan, P.; Shan, H.; Liu, T.; Pei, X.; Wang, G.; Liu, B.; Kalra, M.K.; Xu, X.G. A method of rapid quantification of patient-specific organ doses for CT using deep-learning-based multi-organ segmentation and GPU-accelerated Monte Carlo dose computing. *Med. Phys.* **2020**, *47*, 2526–2536.
50. Gotz, T.I.; Schmidkonz, C.; Chen, S.; Al-Baddai, S.; Kuwert, T.; Lang, E.W. A deep learning approach to radiation dose estimation. *Phys. Med. Biol.* **2019**, *65*, 035007.
51. Kaplan, S.; Zhu, Y.M. Full-Dose PET Image Estimation from Low-Dose PET Image Using Deep Learning: A Pilot Study. *J. Digit. Imaging* **2019**, *32*, 773–778.
52. Roser, P.; Zhong, X.; Birkhold, A.; Strobel, N.; Kowarschik, M.; Fahrig, R.; Maier, A. Physics-driven learning of x-ray skin dose distribution in interventional procedures. *Med. Phys.* **2019**, *46*, 4654–4665.
53. Meineke, A.; Rubbert, C.; Sawicki, L.M.; Thomas, C.; Klosterkemper, Y.; Appel, E.; Caspers, J.; Bethge, O.T.; Kropil, P.; Antoch, G.; Boos, J. Potential of a machine-learning model for dose optimization in CT quality assurance. *Eur. Radiol.* **2019**, *29*, 3705–3713.

54. Gong, K.; Guan, J.; Liu, C.; Qi, J. PET Image Denoising Using a Deep Neural Network Through Fine Tuning. *IEEE Trans. Radiat. Plasma Med. Sci.* **2019**, *3*, 153–161.
55. Xie, S.; Zheng, X.; Chen, Y.; Xie, L.; Liu, J.; Zhang, Y.; Yan, J.; Zhu, H.; Hu, Y. Artifact Removal using Improved GoogLeNet for Sparse-view CT Reconstruction. *Sci. Rep.* **2018**, *8*, 1–9.
56. Han, X. MR-based synthetic CT generation using a deep convolutional neural network method. *Med. Phys.* **2017**, *44*, 1408–1419.
57. Kleesiek, J.; Morshuis, J.N.; Isensee, F.; Deike-Hofmann, K.; Paech, D.; Kickingereeder, P.; Köthe, U.; Rother, C.; Forsting, M.; Wick, W.; et al. Can Virtual Contrast Enhancement in Brain MRI Replace Gadolinium: A Feasibility Study. *Investig. Radiol.* **2019**, *54*, 653–660.
58. Litjens, G.; Kooi, T.; Bejnordi, B.E.; Setio, A.A.A.; Ciompi, F.; Ghafoorian, M.; van der Laak, J.A.W.M.; van Ginneken, B.; Sanchez, C.I. A survey on deep learning in medical image analysis. *Med. Image Anal.* **2017**, *42*, 60–88.
59. Kesner, A.; Schmidtlein, C.R.; Kuntner, C. Real-time data-driven motion correction in PET. *EJNMMI Phys.* **2019**, *6*, 3.
60. Li, M.; Fu, S.; Zhu, Y.; Liu, Z.; Chen, S.; Lu, L.; Liang, C. Computed tomography texture analysis to facilitate therapeutic decision making in hepatocellular carcinoma. *Oncotarget* **2016**, *7*, 13248–13259.
61. Yu, J.Y.; Zhang, H.P.; Tang, Z.Y.; Zhou, J.; He, X.J.; Liu, Y.Y.; Liu, X.J.; Guo, D.J. Value of texture analysis based on enhanced MRI for predicting an early therapeutic response to transcatheter arterial chemoembolisation combined with high-intensity focused ultrasound treatment in hepatocellular carcinoma. *Clin. Radiol.* **2018**, *73*, 758.e9–758.e18.
62. Iezzi, R.; Goldberg, S.N.; Merlino, B.; Posa, A.; Valentini, V.; Manfredi, R. Artificial Intelligence in Interventional Radiology: A Literature Review and Future Perspectives. *J. Oncol.* **2019**, *2019*, 6153041.
63. van Timmeren, J.E.; van Elmpt, W.; Leijenaar, R.T.H.; Reymen, B.; Monshouwer, R.; Bussink, J.; Paelinck, L.; Bogaert, E.; de Wagter, C.; Elhaseen, E.; et al. Longitudinal radiomics of cone-beam CT images from non-small cell lung cancer patients: Evaluation of the added prognostic value for overall survival and locoregional recurrence. *Radiother. Oncol.* **2019**, *136*, 78–85.
64. Rahmim, A.; Huang, P.; Shenkov, N.; Fotouhi, S.; Davoodi-Bojd, E.; Lu, L.; Mari, Z.; Soltanian-Zadeh, H.; Sossi, V. Improved prediction of outcome in Parkinson’s disease using radiomics analysis of longitudinal DAT SPECT images. *Neuroimage Clin.* **2017**, *16*, 539–544.
65. Moraru, A.D.; Costin, D.; Moraru, R.L.; Branisteanu, D.C. Artificial intelligence and deep learning in ophthalmology—Present and future (Review). *Exp. Ther. Med.* **2020**, *20*, 3469–3473.
66. Ricciardi, C.; Cantoni, V.; Improta, G.; Iuppariello, L.; Latessa, I.; Cesarelli, M.; Triassi, M.; Cuocolo, A. Application of data mining in a cohort of Italian subjects undergoing myocardial perfusion imaging at an academic medical center. *Comput. Methods Progr. Biomed.* **2020**, *189*, 105343.
67. Moccia, S.; Banali, R.; Martini, C.; Muscogiuri, G.; Pontone, G.; Pepi, M.; Caiani, E.G. Development and testing of a deep learning-based strategy for scar segmentation on CMR-LGE images. *MAGMA Magn. Reson. Mater. Phys. Biol. Med.* **2018**, *32*, 187–195.
68. Stoel, B. Use of artificial intelligence in imaging in rheumatology—Current status and future perspectives. *RMD Open* **2020**, *6*, e001063, doi:10.1136/rmdopen-2019-001063.
69. Bera, K.; Schalper, K.A.; Rimm, D.L.; Velcheti, V.; Madabhushi, A. Artificial intelligence in digital pathology—New tools for diagnosis and precision oncology. *Nat. Rev. Clin. Oncol.* **2019**, *16*, 703–715.
70. Piehowski, P.D.; Zhu, Y.; Bramer, L.M.; Stratton, K.G.; Zhao, R.; Orton, D.J.; Moore, R.J.; Yuan, J.; Mitchell, H.D.; Gao, Y.; et al. Automated mass spectrometry imaging of over 2000 proteins from tissue sections at 100- $\mu$ m spatial resolution. *Nat. Commun.* **2020**, *11*, 8.
71. Alexandrov, T. Spatial Metabolomics and Imaging Mass Spectrometry in the Age of Artificial Intelligence. *Annu. Rev. Biomed. Data Sci.* **2020**, *3*, 61–87.
72. Voulodimos, A.; Doulamis, N.; Doulamis, A.; Protopapadakis, E. Deep Learning for Computer Vision: A Brief Review. *Comput. Intell. Neurosci.* **2018**, *2018*, 7068349.
73. Cai, T.; Giannopoulos, A.A.; Yu, S.; Kelil, T.; Ripley, B.; Kumamaru, K.K.; Rybicki, F.J.; Mitsouras, D. Natural Language Processing Technologies in Radiology Research and Clinical Applications. *Radiographics* **2016**, *36*, 176–191.
74. Zaharchuk, G.; Gong, E.; Wintermark, M.; Rubin, D.; Langlotz, C.P. Deep Learning in Neuroradiology. *Am. J. Neuroradiol.* **2018**, *39*, 1776–1784.
75. Vávra, P.; Roman, J.; Zonča, P.; Ihnát, P.; Němec, M.; Kumar, J.; Habib, N.; El-Gendi, A. Recent Development of Augmented Reality in Surgery: A Review. *J. Health Eng.* **2017**, *2017*, 4574172.
76. Cheng, Q.; Roelofs, E.; Ramaekers, B.L.; Eekers, D.; van Soest, J.; Lustberg, T.; Hendriks, T.; Hoebbers, F.; van der Laan, H.P.; Korevaar, E.W.; et al. Development and evaluation of an online three-level proton vs photon decision support prototype for head and neck cancer—Comparison of dose, toxicity and cost-effectiveness. *Radiother. Oncol.* **2016**, *118*, 281–285.
77. Lustberg, T.; van Soest, J.; Gooding, M.; Peressutti, D.; Aljabar, P.; van der Stoep, J.; van Elmpt, W.; Dekker, A. Clinical evaluation of atlas and deep learning based automatic contouring for lung cancer. *Radiother. Oncol.* **2018**, *126*, 312–317.
78. Cagni, E.; Botti, A.; Micera, R.; Galeandro, M.; Sghedoni, R.; Orlandi, M.; Iotti, C.; Cozzi, L.; Iori, M. Knowledge-based treatment planning: An inter-technique and inter-system feasibility study for prostate cancer. *Phys. Med.* **2017**, *36*, 38–45.
79. Cagni, E.; Botti, A.; Wang, Y.; Iori, M.; Petit, S.F.; Heijmen, B.J.M. Pareto-optimal plans as ground truth for validation of a commercial system for knowledge-based DVH-prediction. *Phys. Med.* **2018**, *55*, 98–106.

80. Stanhope, C.; Wu, Q.J.; Yuan, L.; Liu, J.; Hood, R.; Yin, F.F.; Adamson, J. Utilizing knowledge from prior plans in the evaluation of quality assurance. *Phys. Med. Biol.* **2015**, *60*, 4873–4891.
81. Nicolae, A.; Semple, M.; Lu, L.; Smith, M.; Chung, H.; Loblaw, A.; Morton, G.; Mendez, L.C.; Tseng, C.L.; Davidson, M.; et al. Conventional vs machine learning-based treatment planning in prostate brachytherapy: Results of a Phase I randomized controlled trial. *Brachytherapy* **2020**, *19*, 470–476.
82. Barragan-Montero, A.M.; Nguyen, D.; Lu, W.; Lin, M.H.; Norouzi-Kandalan, R.; Geets, X.; Sterpin, E.; Jiang, S. Three-dimensional dose prediction for lung IMRT patients with deep neural networks: Robust learning from heterogeneous beam configurations. *Med. Phys.* **2019**, *46*, 3679–3691.
83. Nguyen, D.; Jia, X.; Sher, D.; Lin, M.; Iqbal, Z.; Liu, H.; Jiang, S. 3D radiotherapy dose prediction on head and neck cancer patients with a hierarchically densely connected U-net deep learning architecture. *Phys. Med. Biol.* **2019**, *64*, 065020.
84. Mao, X.; Pineau, J.; Keyes, R.; Enger, S.A. RapidBrachyDL: Rapid Radiation Dose Calculations in Brachytherapy via Deep Learning. *Int. J. Radiat. Oncol.* **2020**, *108*, 802–812.
85. Avanzo, M.; Pirrone, G.; Mileto, M.; Massarut, S.; Stancanello, J.; Baradaran-Ghahfarokhi, M.; Rink, A.; Barresi, L.; Vinante, L.; Piccoli, E.; et al. Prediction of skin dose in low-kV intraoperative radiotherapy using machine learning models trained on results of in vivo dosimetry. *Med. Phys.* **2019**, *46*, 1447–1454.
86. Avanzo, M.; Pirrone, G.; Vinante, L.; Caroli, A.; Stancanello, J.; Drigo, A.; Massarut, S.; Mileto, M.; Urbani, M.; Trovo, M.; et al. Electron Density and Biologically Effective Dose (BED) Radiomics-Based Machine Learning Models to Predict Late Radiation-Induced Subcutaneous Fibrosis. *Front. Oncol.* **2020**, *10*, 490.
87. Talamonti, C.; Piffer, S.; Greto, D.; Mangoni, M.; Ciccarone, A.; Dicarolo, P.; Fantacci, M.E.; Fusi, F.; Oliva, P.; Palumbo, L.; et al. Radiomic and Dosimetric Profiling of Paediatric Medulloblastoma Tumours Treated with Intensity Modulated Radiation Therapy. *Commun. Comput. Inf. Sci.* **2019**, 56–64.
88. Shi, L.; Rong, Y.; Daly, M.; Dyer, B.A.; Benedict, S.; Qiu, J.; Yamamoto, T. Cone-beam computed tomography-based delta-radiomics for early response assessment in radiotherapy for locally advanced lung cancer. *Phys. Med. Biol.* **2020**, *65*, 015009.
89. Guidi, G.; Maffei, N.; Meduri, B.; D'Angelo, E.; Mistretta, G.M.; Ceroni, P.; Ciarmatori, A.; Bernabei, A.; Maggi, S.; Cardinali, M.; et al. A machine learning tool for re-planning and adaptive RT: A multicenter cohort investigation. *Phys. Med.* **2016**, *32*, 1659–1666.
90. Peeken, J.C.; Bernhofer, M.; Wiestler, B.; Goldberg, T.; Cremers, D.; Rost, B.; Wilkens, J.J.; Combs, S.E.; Nusslin, F. Radiomics in radiooncology—Challenging the medical physicist. *Phys. Med.* **2018**, *48*, 27–36.
91. Arabi, H.; Zaidi, H. Applications of artificial intelligence and deep learning in molecular imaging and radiotherapy. *Eur. J. Hybrid Imaging* **2020**, *4*, 17.
92. Placidi, L.; Lenkiewicz, J.; Cusumano, D.; Boldrini, L.; Dinapoli, N.; Valentini, V. Stability of dosimetric features extraction on grid resolution and algorithm for radiotherapy dose calculation. *Phys. Med.* **2020**, *77*, 30–35.
93. Delis, H.; Christaki, K.; Healy, B.; Loreti, G.; Poli, G.L.; Toroi, P.; Meghziene, A. Moving beyond quality control in diagnostic radiology and the role of the clinically qualified medical physicist. *Phys. Med.* **2017**, *41*, 104–108.
94. Kalet, A.M.; Luk, S.M.H.; Phillips, M.H. Radiation Therapy Quality Assurance Tasks and Tools: The Many Roles of Machine Learning. *Med. Phys.* **2020**, *47*, e168–e177.
95. Kimura, Y.; Kadoya, N.; Tomori, S.; Oku, Y.; Jingu, K. Error detection using a convolutional neural network with dose difference maps in patient-specific quality assurance for volumetric modulated arc therapy. *Phys. Med.* **2020**, *73*, 57–64.
96. Li, Q.; Chan, M.F. Predictive time-series modeling using artificial neural networks for Linac beam symmetry: An empirical study. *Ann. N. Y. Acad. Sci.* **2017**, *1387*, 84–94.
97. El Naqa, I.; Irrer, J.; Ritter, T.A.; DeMarco, J.; Al-Hallaq, H.; Booth, J.; Kim, G.; Alkhatib, A.; Popple, R.; Perez, M.; et al. Machine learning for automated quality assurance in radiotherapy: A proof of principle using EPID data description. *Med Phys.* **2019**, *46*, 1914–1921.
98. Nyflot, M.J.; Thammasorn, P.; Wootton, L.S.; Ford, E.C.; Chaovalitwongse, W.A. Deep learning for patient-specific quality assurance: Identifying errors in radiotherapy delivery by radiomic analysis of gamma images with convolutional neural networks. *Med. Phys.* **2019**, *46*, 456–464.
99. Valdes, G.; Chan, M.F.; Lim, S.B.; Scheuermann, R.; Deasy, J.O.; Solberg, T.D. IMRT QA using machine learning: A multi-institutional validation. *J. Appl. Clin. Med. Phys.* **2017**, *18*, 279–284.
100. Bizzego, A.; Bussola, N.; Chierici, M.; Maggio, V.; Francescato, M.; Cima, L.; Cristoforetti, M.; Jurman, G.; Furlanello, C. Evaluating reproducibility of AI algorithms in digital pathology with DAPPER. *PLoS Comput. Biol.* **2019**, *15*, e1006269.
101. Shaikhina, T.; Lowe, D.; Daga, S.; Briggs, D.; Higgins, R.; Khovanova, N. Machine Learning for Predictive Modelling based on Small Data in Biomedical Engineering. *IFAC-PapersOnLine* **2015**, *48*, 469–474.
102. Chatterjee, A.; Vallières, M.; Dohan, A.; Levesque, I.R.; Ueno, Y.; Bist, V.; Saif, S.; Reinhold, C.; Seuntjens, J. An Empirical Approach for Avoiding False Discoveries When Applying High-Dimensional Radiomics to Small Datasets. *IEEE Trans. Radiat. Plasma Med. Sci.* **2019**, *3*, 201–209.
103. Cui, S.; Tseng, H.H.; Pakela, J.; Haken, R.K.T.; El Naqa, I. Introduction to machine and deep learning for medical physicists. *Med. Phys.* **2020**, *47*, e127–e147.
104. Stepwise Regression, F.G.R. *Anonymous Wiley International Encyclopedia of Marketing*; American Cancer Society: Atlanta, GA, USA, 2010.

105. Parmar, C.; Grossmann, P.; Rietveld, D.; Rietbergen, M.M.; Lambin, P.; Aerts, H.J. Radiomic Machine-Learning Classifiers for Prognostic Biomarkers of Head and Neck Cancer. *Front. Oncol.* **2015**, *5*, 272.
106. Lian, C.; Ruan, S.; Denooux, T.; Jardin, F.; Vera, P. Selecting radiomic features from FDG-PET images for cancer treatment outcome prediction. *Med. Image Anal.* **2016**, *32*, 257–268.
107. Wu, W.; Parmar, C.; Grossmann, P.; Quackenbush, J.; Lambin, P.; Bussink, J.; Mak, R.; Aerts, H.J. Exploratory Study to Identify Radiomics Classifiers for Lung Cancer Histology. *Front. Oncol.* **2016**, *6*, 71.
108. Hinton, G.E.; Srivastava, N.; Krizhevsky, A.; Sutskever, I.; Salakhutdinov, R.R. Improving neural networks by preventing co-adaptation of feature detectors, *arXiv* **2012**, arXiv:1207.0580.
109. Lemaitre, G.; Nogueira, F.; Aridas, C.K. Imbalanced-learn: A Python Toolbox to Tackle the Curse of Imbalanced Datasets in Machine Learning. *arXiv* **2016**, arXiv:1609.06570.
110. Buda, M.; Maki, A.; Mazurowski, M.A. A systematic study of the class imbalance problem in convolutional neural networks. *arXiv* **2017**, arXiv:1710.05381.
111. Chen, J.H.; Alagappan, M.; Goldstein, M.K.; Asch, S.M.; Altman, R.B. Decaying relevance of clinical data towards future decisions in data-driven inpatient clinical order sets. *Int. J. Med. Inform.* **2017**, *102*, 71–79.
112. Nensa, F.; Demircioglu, A.; Rischpler, C. Artificial Intelligence in Nuclear Medicine. *J. Nucl. Med.* **2019**, *60*, 29S–37S.
113. Li, H.; Zhu, Y.; Burnside, E.S.; Drukker, K.; Hoadley, K.A.; Fan, C.; Conzen, S.D.; Whitman, G.J.; Sutton, E.J.; Net, J.M.; et al. MR Imaging Radiomics Signatures for Predicting the Risk of Breast Cancer Recurrence as Given by Research Versions of MammaPrint, Oncotype DX, and PAM50 Gene Assays. *Radiology* **2016**, *281*, 382–391.
114. Aerts, H.J.; Grossmann, P.; Tan, Y.; Oxnard, G.G.; Rizvi, N.; Schwartz, L.H.; Zhao, B. Defining a Radiomic Response Phenotype: A Pilot Study using targeted therapy in NSCLC. *Sci. Rep.* **2016**, *6*, 33860.
115. Geis, J.R.; Brady, A.P.; Wu, C.C.; Spencer, J.; Ranschaert, E.; Jaremko, J.L.; Langer, S.G.; Kitts, A.B.; Birch, J.; Shields, W.F. et al. Ethics of Artificial Intelligence in Radiology: Summary of the Joint European and North American Multisociety Statement. *Can. Assoc. Radiol. J.* **2019**, *70*, 329–334.
116. Lai, M.C.; Brian, M.; Mamzer, M.F. Perceptions of artificial intelligence in healthcare: Findings from a qualitative survey study among actors in France. *J. Transl. Med.* **2020**, *18*, 1–13.
117. Pesapane, F.; Codari, M.; Sardanelli, F. Artificial intelligence in medical imaging: Threat or opportunity? Radiologists again at the forefront of innovation in medicine. *Eur. Radiol. Exp.* **2018**, *2*, 1–10.
118. Townsend, D.; Cheng, Z.; Georg, D.; Drexler, W.; Moser, E. Grand challenges in biomedical physics. *Front. Phys.* **2013**, *1*, 1.
119. Sensakovic, W.F.; Mahesh, M. Role of the Medical Physicist in the Health Care Artificial Intelligence Revolution. *J. Am. Coll. Radiol.* **2019**, *16*, 393–394.
120. Cody, D.D.; Fisher, T.S.; Gress, D.A.; Layman, R.R., Jr.; McNitt-Gray, M.F.; Pizzutiello, R.J., Jr.; Fairbent, L.A. AAPM medical physics practice guideline 1.a: CT protocol management and review practice guideline. *J. Appl. Clin. Med Phys.* **2013**, *14*, 3–12.
121. Mackin, D.; Fave, X.; Zhang, L.; Fried, D.; Yang, J.; Taylor, B.; Rodriguez-Rivera, E.; Dodge, C.; Jones, A.K.; Court, L. Measuring Computed Tomography Scanner Variability of Radiomics Features. *Investig. Radiol.* **2015**, *50*, 757–765.
122. Fave, X.; Cook, M.; Frederick, A.; Zhang, L.; Yang, J.; Fried, D.; Stingo, F.; Court, L. Preliminary investigation into sources of uncertainty in quantitative imaging features. *Comput. Med. Imaging Graph.* **2015**, *44*, 54–61.
123. Samei, E.; Hoye, J.; Zheng, Y.; Solomon, J.B.; Marin, D. Design and fabrication of heterogeneous lung nodule phantoms for assessing the accuracy and variability of measured texture radiomics features in CT. *J. Med. Imaging* **2019**, *6*, 021606.
124. Pfaehler, E.; Beukinga, R.J.; de Jong, J.R.; Slart, R.H.J.A.; Slump, C.H.; Dierckx, R.A.J.O.; Boellaard, R. Repeatability of (18) F-FDG PET radiomic features: A phantom study to explore sensitivity to image reconstruction settings, noise, and delineation method. *Med. Phys.* **2019**, *46*, 665–678.
125. Bianchini, L.; Botta, F.; Origgi, D.; Rizzo, S.; Mariani, M.; Summers, P.; García-Polo, P.; Cremonesi, M.; Lascialfari, A. PETER PHAN: An MRI phantom for the optimisation of radiomic studies of the female pelvis. *Phys. Med.* **2020**, *71*, 71–81.
126. Kim, H.; Park, C.M.; Lee, M.; Park, S.J.; Song, Y.S.; Lee, J.H.; Hwang, E.J.; Goo, J.M. Impact of Reconstruction Algorithms on CT Radiomic Features of Pulmonary Tumors: Analysis of Intra- and Inter-Reader Variability and Inter-Reconstruction Algorithm Variability. *PLoS ONE.* **2016**, *11*, e0164924.
127. Leijenaar, R.T.; Carvalho, S.; Velazquez, E.R.; van Elmpt, W.J.; Parmar, C.; Hoekstra, O.S.; Hoekstra, C.J.; Boellaard, R.; Dekker, A.L.; Gillies, R.J.; et al. Stability of FDG-PET Radiomics features: An integrated analysis of test-retest and inter-observer variability. *Acta Oncol.* **2013**, *52*, 1391–1397.
128. Zhao, B.; James, L.P.; Moskowitz, C.S.; Guo, P.; Ginsberg, M.S.; Lefkowitz, R.A.; Qin, Y.; Riely, G.J.; Kris, M.G.; Schwartz, L.H. Evaluating Variability in Tumor Measurements from Same-day Repeat CT Scans of Patients with Non-“Small Cell Lung Cancer. *Radiology* **2009**, *252*, 263–272.
129. Desseroit, M.C.; Tixier, F.; Weber, W.A.; Siegel, B.A.; le Rest, C.C.; Visvikis, D.; Hatt, M. Reliability of PET/CT shape and heterogeneity features in functional and morphological components of Non-Small Cell Lung Cancer tumors: A repeatability analysis in a prospective multi-center cohort. *J. Nucl. Med.* **2016**, *58*, 406–411.
130. Galavis, P.E.; Hollensen, C.; Jallow, N.; Paliwal, B.; Jeraj, R. Variability of textural features in FDG PET images due to different acquisition modes and reconstruction parameters. *Acta Oncol.* **2010**, *49*, 1012–1016.
131. Lu, L.; Lv, W.; Jiang, J.; Ma, J.; Feng, Q.; Rahmim, A.; Chen, W. Robustness of Radiomic Features in [11C]Choline and [18F]FDG PET/CT Imaging of Nasopharyngeal Carcinoma: Impact of Segmentation and Discretization. *Mol. Imaging Biol.* **2016**, *18*, 935–945.



132. Bailly, C.; Bodet-Milin, C.; Couespel, S.; Necib, H.; Kraeber-Bodéré, F.; Ansquer, C.; Carlier, T. Revisiting the robustness of PET-based textural features in the context of multi-centric trials. *PLoS ONE* **2016**, *11*, e0159984.
133. Yang, F.; Dogan, N.; Stoyanova, R.; Ford, J.C. Evaluation of radiomic texture feature error due to MRI acquisition and reconstruction: A simulation study utilizing ground truth. *Phys. Med.* **2018**, *50*, 26–36.
134. Kaus, M.R.; Brock, K.K.; Pekar, V.; Dawson, L.A.; Nichol, A.M.; Jaffray, D.A. Assessment of a model-based deformable image registration approach for radiation therapy planning. *Int. J. Radiat. Oncol.* **2007**, *68*, 572–580.
135. Isaksson, L.J.; Raimondi, S.; Botta, F.; Pepa, M.; Gugliandolo, S.G.; de Angelis, S.P.; Marvaso, G.; Petralia, G.; de Cobelli, O.; Gandini, S.; et al. Effects of MRI image normalization techniques in prostate cancer radiomics. *Phys. Med.* **2020**, *71*, 7–13.
136. Brock, K.K. Deformable Registration Accuracy Consortium, Results of a multi-institution deformable registration accuracy study (MIDRAS). *Int. J. Radiat. Oncol.* **2010**, *76*, 583–596.
137. Avanzo, M.; Barbiero, S.; Trovo, M.; Bissonnette, J.P.; Jena, R.; Stancanello, J.; Pirrone, G.; Matrone, F.; Minatel, E.; Cappelletto, C.; et al. Voxel-by-voxel correlation between radiologically radiation induced lung injury and dose after image-guided, intensity modulated radiotherapy for lung tumors. *Phys. Med.* **2017**, *42*, 150–156.
138. Mahesh, M. Essential Role of a Medical Physicist in the Radiology Department. *Radiographics* **2018**, *38*, 1665–1671.
139. Herrmann, M.D.; Clunie, D.A.; Fedorov, A.; Doyle, S.W.; Pieper, S.; Klepeis, V.; Le, L.P.; Mutter, G.L.; Milstone, D.S.; Schultz, T.J.; et al. Implementing the DICOM Standard for Digital Pathology. *J. Pathol. Inform.* **2018**, *9*, 37.
140. Kortensniemi, M.; Tsapaki, V.; Trianni, A.; Russo, P.; Maas, A.; Kallman, H.E.; Brambilla, M.; Damilakis, J. The European Federation of Organisations for Medical Physics (EFOMP) White Paper: Big data and deep learning in medical imaging and in relation to medical physics profession. *Phys. Med.* **2018**, *56*, 90–93.
141. Zwanenburg, A.; Leger, S.; Vallieres, M.; Lock, S. theImage Biomarker Standardisation Initiative for, Image biomarker standardisation initiative. *arXiv* **2016**, arXiv:1612.07003.
142. Mahon, R.N.; Ghita, M.; Hugo, G.D.; Weiss, E. ComBat harmonization for radiomic features in independent phantom and lung cancer patient computed tomography datasets. *Phys. Med. Biol.* **2019**, *65*, 015010.
143. Kesner, A.; Laforest, R.; Otazo, R.; Jennifer, K.; Pan, T. Medical imaging data in the digital innovation age. *Med. Phys.* **2018**, *45*, e40–e52.
144. Parmar, C.; Grossmann, P.; Bussink, J.; Lambin, P.; Aerts, H.J. Machine Learning methods for Quantitative Radiomic Biomarkers. *Sci. Rep.* **2015**, *5*, 13087.
145. Barucci, A. Adversarial radiomics: The rising of potential risks in medical imaging from adversarial learning. *Eur. J. Nucl. Med. Mol. Imaging* **2020**, *47*, 2941–2943.
146. Li, S.; Chen, Y.; Peng, Y.; Bai, L. Learning More Robust Features with Adversarial Training. *arXiv* **2018**, arXiv:1804.07757.
147. U.S. Food and Drug Administration: MicroArray/Sequencing Quality Control (MAQC/SEQC). 2021. Available online: <https://www.fda.gov/science-research/bioinformatics-tools/microarraysequencing-quality-control-maqcseqc> (accessed on 12 February 2021).
148. Collins, G.S.; Reitsma, J.B.; Altman, D.G.; Moons, K.G. Transparent reporting of a multivariable prediction model for individual prognosis or diagnosis (TRIPOD): The TRIPOD Statement. *MC Med.* **2015**, *13*, 1–10.
149. Wang, B.; White, G. The role of clinical medical physicists in the future: Quality, safety, technology implementation, and enhanced direct patient care. *J. Appl. Clin. Med. Phys.* **2019**, *20*, 4–6.
150. Caruana, C.J.; Tsapaki, V.; Damilakis, J.; Brambilla, M.; Martin, G.M.; Dimov, A.; Bosmans, H.; Egan, G.; Bacher, K.; McClean, B. EFOMP policy statement 16: The role and competences of medical physicists and medical physics experts under 2013/59/EURATOM. *Phys. Med.* **2018**, *48*, 162–168.
151. Okamoto, H.; Ota, S.; Kawamorita, R.; Sakamoto, M.; Nakamura, S.; Nishioka, S.; Kabuki, S.; Masai, N.; Mizuno, N.; Furuya, T.; et al. Summary of the Report of Task Group 100 of the AAPM: Application of Risk Analysis Methods to Radiation Therapy Quality Management. *Igaku Butsuri* **2020**, *40*, 28–34.
152. Bang, J.Y.; Hough, M.; Hawes, R.H.; Varadarajulu, S. Use of Artificial Intelligence to Reduce Radiation Exposure at Fluoroscopy-Guided Endoscopic Procedures. *Am. J. Gastroenterol.* **2020**, *115*, 555–561.
153. Liu, Y.; Ma, L.; Zhao, J. Secure Deep Learning Engineering: A Road Towards Quality Assurance of Intelligent Systems. In *Lecture Notes in Computer Science*; Springer: Berlin, Germany, 2019; pp. 3–15.
154. Tang, A.; Tam, R.; Cadrin-Chênevert, A.; Guest, W.; Chong, J.; Barfett, J.; Chepelev, L.; Cairns, R.; Mitchell, J.R.; Cicero, M.D.; et al. Canadian Association of Radiologists White Paper on Artificial Intelligence in Radiology. *Can. Assoc. Radiol. J.* **2018**, *69*, 120–135.
155. Currie, G.; Hawk, K.E.; Rohren, E.; Vial, A.; Klein, R. Machine Learning and Deep Learning in Medical Imaging: Intelligent Imaging. *J. Med Imaging Radiat. Sci.* **2019**, *50*, 477–487.
156. Prior, F.W.; Clark, K.; Commean, P.; Freymann, J.; Jaffe, C.; Kirby, J.; Moore, S.; Smith, K.; Tarbox, L.; Vendt, B.; et al. TCIA: An information resource to enable open science. *Conf. Proc. IEEE Eng. Med. Biol. Soc.* **2013**, *2013*, 1282–1285.
157. Sharma, A.; Tarbox, L.; Kurc, T.; Bona, J.; Smith, K.; Kathiravelu, P.; Bremer, E.; Saltz, J.H.; Prior, F. PRISM: A Platform for Imaging in Precision Medicine. *JCO Clin. Cancer Inform.* **2020**, *4*, 491–499.
158. Wilkinson, M.D.; Dumontier, M.; Aalbersberg, I.J.; Appleton, G.; Axton, M.; Baak, A.; Blomberg, N.; Boiten, J.W.; Santos, L.B.D.; The FAIR Guiding Principles for scientific data management and stewardship. *Sci. Data* **2016**, *3*, 160018.